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1 Abstract

2

3 Background

4 Cervical dystonia (CD) is a movement disorder characterized by involuntary muscle contractions
5 leading to an abnormal head posture or movements of the neck. Dysfunctions in somatosensory
6 integration are present and previous data showed enlarged postural sway in stance.

7 Objectives

8 To investigate postural control during quiet sitting and the correlation with cervical sensorimotor
9 control.

10 Method

11 Postural control during quiet sitting was measured via body sway parameters in 23 patients with CD,
12 regularly receiving botulinum toxin treatment and compared with 36 healthy controls. Amplitude
13 and velocity of displacements of the Center of Pressure (CoP) were measured by 2 embedded force
14 plates at 1000Hz. Three samples of 30 seconds were recorded with the eyes open and closed.
15 Disease specific characteristics were obtained in all patients by the Tsui scale, Cervical Dystonia
16 Impact Profile (CDIP-58) and Toronto Western Spasmodic Rating Scale (TWSTRS). Cervical
17 sensorimotor control was assessed with an infrared Vicon system during a head repositioning task.

18 Results

19 Body sway amplitude and velocity were increased in patients with CD compared to healthy controls.
20 CoP displacements were doubled in patients without head tremor and tripled in patients with a
21 dystonic head tremor. Impairments in cervical sensorimotor control were correlated with larger CoP
22 displacements (r_s ranged from 0.608 to 0.748).

23

24 Conclusion

25 Postural control is impaired and correlates with dysfunction in cervical sensorimotor control in
26 patients with CD. Treatment is **currently** focused on the cervical area. Further research towards the
27 potential value of postural control exercises is recommended.

28 Key words: cervical dystonia, sensorimotor integration, postural control, seated balance

29

1 **Introduction**

2 Adult onset idiopathic Cervical Dystonia (CD) is a rare movement disorder. It is a focal
3 dystonia which is characterized by involuntary contractions of neck muscles resulting in an abnormal
4 head posture and neck movement. CD is frequently painful and sometimes accompanied by head
5 tremor (Albanese et al. 2011; Jinnah and Albanese 2014). Treatment of choice is injection with
6 Botulinum Toxin (Albanese et al. 2011) and physical therapy can be used as an adjuvant therapy (De
7 Pauw et al. 2014). The cause of CD remains unknown and in addition to motor symptoms CD is
8 associated with non-motor symptoms such as sleep disorders, sensory deficits, deficits in
9 somatosensory integration such as enlarged temporal and spatial discrimination thresholds (Fiorio et
10 al. 2007; Tinazzi et al. 2009; Avanzino et al. 2010; Patel, Neepa; Jankovic, Joseph; Hallett 2014;
11 Antelmi et al. 2016). Deficits of sensorimotor integration have been observed with motor evoked
12 potentials through transcranial stimulation (Abbruzzese et al. 2001) are thought to play a role in
13 alleviation manoeuvres in which a slight sensory touch alters motor response (Konczak and
14 Abbruzzese 2013; Patel et al. 2014).

15

16 In CD, deficits of sensorimotor integration have been observed related to impaired neck
17 proprioception (Bove et al. 2007; De Pauw et al. 2017a). Impairment in neck proprioception may lead
18 to disturbances in balance and posture (Treleaven et al. 2006; Field et al. 2008; Vuillerme and
19 Pinsault 2009) as well as neck pain and dizziness (Revel M, Minguet M, Gregoy P, Vaillant J 1994;
20 Treleaven et al. 2003; Eva-Maj et al. 2013). Postural control and maintaining balance depends on the
21 incorporation of somatosensory, visual and vestibular afferent information. Body sway increases
22 when one or more sensory stimuli are altered (Peterka 2002). Changes in support surface or motion
23 stimuli as well as alterations in cervical proprioceptive information increase postural sway. For
24 instance, neck muscle vibration in particular or cervical muscular fatigue affects postural steadiness
25 (Bove et al. 2007; Vuillerme and Pinsault 2009). Experimentally induced neck muscle fatigue or neck

1 muscle vibration stimulates sensory receptors in the muscle spindles. Given the high density of
2 muscle spindles in suboccipital muscles, neck proprioception plays an important role in maintaining
3 postural control (Pettorossi and Schieppati 2014).

4

5 Although half of the patients with CD report difficulties with walking (De Pauw et al. 2017b),
6 postural control in CD is not well documented. Alterations in gait stability as well as poor balance
7 performance on functional balance tests such as the timed up and go test have been reported (Barr
8 et al. 2017). Regarding postural steadiness, previous posturographic research in quiet stance shows
9 conflicting results. Two studies reported increased postural sway in quiet stance as shown by
10 enlarged antero-posterior and medio-lateral sway, sway path and area (Wöber et al. 1999; Bove et
11 al. 2007) in a population of patients with and without head tremor. Two other studies observed no
12 difference between healthy controls and patients with CD (Lekhel et al. 1997; Moreau et al. 1999) in
13 a population of patients without tremor. Maintaining postural balance in stance predominantly relies
14 on ankle strategy (Gatev et al. 1999). To minimize somatosensory input from the lower limbs, the aim
15 of this exploratory study was to investigate seated postural control. As neck proprioception plays an
16 important role in maintaining postural control (Pettorossi and Schieppati 2014), the secondary aim
17 was to uncover correlations between seated postural control and cervical sensorimotor control.
18 Additionally, to explore whether disease severity influences postural control, correlations were
19 investigated.

20

21

22

1 **Material and methods**

2

3 1.1 Subject characteristics and clinical assessment

4 In this cross-sectional study, a group of 23 patients with adult-onset idiopathic CD was compared to a
5 group of 36 healthy controls. Patients were recruited at a tertiary care center in the department of
6 Neurology at the Antwerp University Hospital. All patients were diagnosed by an experienced
7 neurologist in accordance with the European Federation of Neurological Societies / Movement
8 Disorders Society European Section (EFNS/MDS-ES) guidelines (Albanese et al. 2011) and received
9 regular treatments of botulinum toxin injections. The assessment took place at least 3 months after
10 the last injection, immediately prior to a new injection of botulinum toxin. Patients were excluded in
11 case of clinical features suggestive for segmental distribution of dystonia, other neurological
12 disorders, vestibular dysfunction, or previous surgery of the cervical spine and alcohol intake in the
13 last 24 hours.

14 Clinical assessment of the CD symptoms was performed using 3 disease specific rating scales: the
15 Cervical Dystonia Impact Profile (CDIP-58) and Toronto Western Spasmodic Rating Scale (TWSTRS) for
16 disease severity and the tremor subscale of the Tsui scale for the assessment of the dystonic head
17 tremor.

18 The protocol was approved by the Ethics Committee of the Antwerp University Hospital (reference
19 14/8/74) and all participants provided written informed consent. The assessment was performed in
20 the Multidisciplinary Motor Centre Antwerp (M²OCEAN).

21

22 1.2 Measurements

23 **Seated postural control** was assessed during quiet sitting with 2 embedded force plates (AMTI®,
24 Advanced Mechanical Technology Inc., Watertown, MA). Center of Pressure (CoP) displacement was

1 measured with a sampling frequency of 1000Hz and filtered through a 4th order zero phase
2 Butterworth lowpass filter with a cut-off frequency of 10Hz (Latash et al. 2003). Participants were
3 seated on a chair without back or arm rests on one force plate (see Fig.1). Both feet were placed next
4 to each other with the hands resting on the thighs on the adjacent force plate. The force plates
5 generated 3 force components, Fx, Fy and Fz and 3 components of the moment of force acting on the
6 force plate Mx, My, Mz (x, y and z are the anterior-posterior, medial-lateral and vertical directions,
7 respectively). The signals were processed with Vicon[®] software (version 1.8.5). A custom made
8 Matlab model was written to calculate CoP parameters in which total CoP was calculated as the
9 weighted average of the CoP displacements on the 2 force plates. Following CoP parameters as
10 previously described by Prieto et al. (Prieto et al. 1996) were calculated: range of the antero-
11 posterior and mediolateral displacements (mm) (range ML, range AP), CoP path as distance covered
12 by the successive positions of the moving CoP (mm), the area (mm²) of an ellipse which encompassed
13 95% of the CoP distribution and the mean velocity of CoP displacements in the antero-posterior and
14 medio-lateral direction (mm/s) (mVel ML and mVel AP). Three samples of 30 seconds were recorded
15 with the eyes closed and eyes open (Duarte and Freitas 2010) with a 30s rest between trials. To
16 increase reliability, the first 10 s of each trial were discarded to avoid fluctuations in CoP and non-
17 stationarity start of the measurement (Carpenter et al. 2001).

18 PLEASE INSERT FIG.1 ABOUT HERE

19

20 **Cervical sensorimotor control** was evaluated by joint position error (JPE) in the head
21 repositioning accuracy (HRA) test, which was measured in degrees (°). Measurements were obtained
22 through 3D motion analysis using an infrared camera system with 8 cameras recording at 100 Hz
23 (VICON[®] T10, Oxford Metrics, Oxford). Rigid plates with reflective markers were placed on the head
24 and sternum (See Figure 2). No alleviating effect was reported of the pressure of the head band in
25 the patient group. In the HRA test, blindfolded participants had to relocate their head as accurately

1 as possible to a self-determined neutral head position (NHP) after performing an active movement
2 (flexion, extension, left and right rotation of the neck) (Revel and Andre-Deshays, Claudie Minguet
3 1991). The NHP for patients was equal to the dystonic head position. This test is proven to be valid
4 and reliable (Michiels et al. 2013). Participants performed 10 repetitions in every movement
5 direction. The captured data of the Vicon® markers were first reconstructed and labelled using
6 Nexus® software. Afterwards, a custom made biomechanical model was used to calculate angle
7 positions for each captured frame. Hence, movement angles of the neck were calculated using XYZ
8 Euler/Cardan rotations of the head segment relative to the sternum segment. These data were then
9 processed, using a custom made MATLAB® code to calculate the JPE (De Pauw et al. 2017a). The
10 absolute JPE, e.g. absolute error (AE), was calculated as the mean difference between the absolute
11 values of the NHP and the position of the head after relocation (Hill et al. 2009). $AE = (absolute\ of$
12 $raw\ error\ trial\ 1) + (absolute\ of\ raw\ error\ trial\ 2) + \dots + (absolute\ of\ raw\ error\ trial\ 10) / 10$. The AE is a
13 measure for cervical sensorimotor control and larger AE indicates poorer cervical sensorimotor
14 control (Röijezon et al. 2015). Comparison was made between the patient group and a normative
15 database of 70 healthy controls.

16 PLEASE INSERT FIGURE 2 ABOUT HERE

17

18 1.3 Statistical analysis

19 Data were analyzed using SPSS® vs. 22. Non-parametric statistical tests were used for the
20 posturographic measures for non-normally distributed data. The level of significance was set at
21 $p < 0.05$ and was adjusted with a post-hoc Bonferroni correction given the multiple outcome
22 parameters. As 6 parameters of postural control were obtained, Bonferroni correction was calculated
23 as $0.05/6 = 0.00833$.

1 As the presence of head tremor could influence cervical sensorimotor control and posturographic
2 measures, the patient group was divided in 2 groups. Group 1 included patients with CD showing no
3 head tremor, group 2 included patients with CD showing a visible dystonic head tremor. Between
4 group differences between the control group and the two patients groups for postural control were
5 analyzed with a Kruskal Wallis test with a post hoc analysis by a Mann-Whitney U test. For cervical
6 sensorimotor control, we found no differences between patients with and without head tremor so a
7 Mann-Whitney U test was used to calculate between group differences in cervical sensorimotor
8 control between the control group and the patient group.

9 Spearman's rho correlations were calculated in the 3 groups first between the JPE as a measure for
10 cervical sensorimotor control and postural sway parameters. Secondly, Spearman's rho correlations
11 were calculated between clinical measures and postural sway parameters.

1 Results

2

3 1.1 Patient characteristics

4 We included 23 patients with adult onset idiopathic CD (3 men, 19 females) with a mean disease
5 duration of 13.0 years (± 8.7 SD) and 36 healthy controls (16 men, 20 females). Of the patients with
6 CD, 11 patients showed a visible dystonic head tremor. The mean age of the patient group (59.4
7 years ± 14.6 , mean \pm SD) and control group (58.9 years ± 16.6 , mean \pm SD) did not differ (unpaired *t*
8 test: $p=0.904$). Patient characteristics are shown in Table 1.

9 PLEASE INSERT TABLE 1 ABOUT HERE

10 Table 1: patient characteristics

Gender	Age (years)	Duration CD (years)	Type of CD	Tremor /4	TWSTRS /85	CDIP-58 /100
F	44	2	Right T + Left La	0	34.87	68.62
M	41	7	Right La	0	29.5	41.03
F	76	14	Right T + Left La + Left Lateral shift	0	44.75	49.66
F	68	15	Left T	0	28.25	36.21
F	35	9	Left T + Re	0	26.75	48.62
F	71	7	Right T + Right La + sagittal shift forward	0	36	41.72
F	58	11	Right T + Left La	4	40.25	42.41
F	62	7	Right T + Left La	0	44.75	67.93
F	61	9,5	Right T + Right La + An	0	56	53.79
F	59	14	Right T + Left La	1	27	41.72
M	71	8	Right T + Right La + sagittal shift backward	0	41.75	34.83
F	30	11	Right T + Right La	4	21.75	25.86
M	43	8	Right T + Right La	0	36.75	44.48
F	70	7	Right T + Left La	0	26.75	30.34
F	55	10	Right T + Right La	1	34.75	50.00
F	70	35	Right T + Right La	4	40.25	75.86
F	86	34	Left T + Right La + An	1	27.25	28.62
F	74	8	Left T + Right La	4	27	42.07
F	48	9	Right T + Right lateral shift	2	46.25	73.45
F	59	17	Left T + Left La	0	61.75	63.10
F	71	31	Left T + Left La + An	1	30.5	38.97
F	50	6	Right T + Right La	0	38.5	55.86
F	64	15	Right T + left La	4	34.125	45.52
mean	59.25	13.02		1.17	36.07	47.69
SD	± 13.96	± 8.72			± 9.74	± 13.79

Legend: M=male, F=female, T=torticollis, CD= cervical dystonia, La=laterocollis, An=anterocollis, Re=retrocollis, TWSTRS=Toronto Western Spasmodic Rating Scale, CDIP-58=Cervical Dystonia Impact Profile, SD= standard deviation Tremor according to Tsui scale: product of severity x duration (severity: 1=light 2=severe and duration 1=intermittent 2= constant)(28)

11

1 1.2 Seated postural control

2 All postural sway parameters were significantly larger in patients with CD compared to controls
 3 ($p < 0.0001$ with Kruskal Wallis test). In the patient group, postural sway parameters of patients with
 4 head tremor were significantly larger compared to patients without head tremor especially in the
 5 eyes open condition (see Table 2). Body sway amplitude and velocity were twice as large in patients
 6 without head tremor compared to controls in the eyes closed condition. In patients with head
 7 tremor, CoP displacements were 3 to 4 times larger compared to displacements in the control group.
 8 No significant differences were observed between the CoP displacements in the condition eyes open
 9 and eyes closed in the control group nor the patient groups. (range ML $p = 0.263$, range AP $p = 0.077$,
 10 path $p = 0.884$, mVel ML $p = 0.408$, mVel AP $p = 0.685$, area $p = 0.077$)
 11 No correlations were observed between posturographic parameters and disease specific
 12 characteristics such as severity of CD ($p = 0.300$), head tilt ($p = 0.546$) nor duration of the disease (p
 13 $= 0.693$).

14 PLEASE INSERT TABLE 2 ABOUT HERE

15
 16 Table 2. Postural sway parameters in seated position, between group analysis based on the presence
 17 of head tremor

		Healthy Controls Group 0 n=36	Patients without Tremor Group 1 n=12	Patients with tremor Group 2 n=11	Between group differences <i>p</i> -value post hoc		
					0 – 1	0 – 2	1 - 2
Eyes open							
Range	ML (mm)	2.53 (2.47)	4.06 (3.30)	8.43 (4.58)	0.001**	<0.0001 **	0.025*
	AP (mm)	3.45 (3.13)	5.30 (5.95)	11.47 (15.33)	0.001**	<0.0001 **	0.030*
Path	(mm)	198.44 (183.86)	289.05 (200.68)	974.55 (728.56)	0.009 *	<0.0001 **	0.002**
Mean	mVel ML (mm/s)	3.56 (3.70)	4.99 (4.30)	11.78 (12.32)	0.060	<0.0001 **	0.002**
Velocity	mVel AP (mm/s)	4.96 (4.07)	7.81 (4.52)	26.17 (22.62)	0.002**	<0.0001 **	0.001**
Area	(mm ²)	2.41 (3.99)	5.60 (7.33)	26.85 (44.20)	0.004**	<0.0001 **	0.017*
Eyes closed							
Range	ML (mm)	2.54 (2.53)	4.97 (3.83)	8.41 (5.15)	0.001**	<0.0001 **	0.107
	AP (mm)	3.27 (3.09)	6.72 (4.22)	10.20 (13.93)	<0.0001**	<0.0001 **	0.140
Path	(mm)	179.43 (177.50)	316.55 (203.06)	656.27 (930.75)	0.003 **	<0.0001 **	0.014*
Mean	mVel ML (mm/s)	3.24 (3.12)	5.48 (4.47)	10.97 (10.82)	0.009*	<0.0001 **	0.030*
Velocity	mVel AP (mm/s)	4.46 (4.19)	7.84 (4.38)	15.94 (29.88)	<0.0001**	<0.0001 **	0.021*
Area	(mm ²)	2.12 (3.96)	8.29 (9.28)	17.98 (43.79)	<0.0001**	<0.0001 **	0.080

median and interquartile range are reported

ML: range of the CoP displacement in medio-lateral direction, AP: range of the CoP displacement in antero-posterior direction

mVel ml: mean velocity of the CoP displacement in medio-lateral direction, mVel ap: mean velocity of the CoP displacement in

antero-posterior direction, Area: area of an ellipse that encompassed 95% of the CoP distribution

* sig at 0.05 level, ** sig after Bonferroni correction $p < 0.01$ ($0.05/6=0.00833$)

1 PLEASE INSERT FIG.3 ABOUT HERE

2

3 1.3 Cervical sensorimotor control

4 The AE was larger in the patient group compared to the control group (Mann-Whitney U test: AE
5 extension: $p= 0.015$, AE flexion: $p = 0.002$, AE left rotation: $p <0.0001$, AE right rotation: $p = 0.0006$).

6 For more detailed information, see De Pauw et al. 2017a.

7

8 1.4 Correlation between cervical sensorimotor control and postural sway

9 The AE was moderately to strongly correlated with postural sway in the patient group without head
10 tremor. Larger joint repositioning errors, i.e. poorer cervical sensorimotor control, correlated with
11 larger CoP parameters (see Table 3). The AE of flexion correlated with all measurements of CoP
12 parameters in the condition eyes closed. The AE of left rotation was positively correlated with the
13 range of antero-posterior CoP displacements and the mean medio-lateral and antero-posterior
14 velocity of CoP displacements. The mean medio-lateral and antero-posterior velocity of CoP
15 displacements remained significant after a Bonferroni correction given the multiple parameters.
16 These correlations were not found in the control group nor the patient group with head tremor. In
17 the condition eyes open, the AE correlated with the same CoP parameters, although less strongly.

18

19 PLEASE INSERT TABLE 3 ABOUT HERE

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1 Table 3. Spearman's rho correlation coefficients between cervical sensorimotor control and CoP
 2 parameters in patients without head tremor in the situation eyes closed.

	Range ML (mm)	Range AP (mm)	Path (mm)	mVel ML (mm/s)	mVel AP (mm/s)	Area (mm ²)
Mean AE extension (°)	0.119	0.329	0.210	0.189	0.315	0.231
<i>p</i> -value	0.713	0.297	0.513	0.557	0.319	0.471
Mean AE flexion (°)	0.643*	0.622*	0.748**	0.713*	0.720**	0.664*
<i>p</i> -value	0.024	0.031	0.005	0.009	0.008	0.018
Mean AE left rotation (°)	0.406	0.720**	0.608*	0.608*	0.622*	0.497
<i>p</i> -value	0.191	0.008	0.036	0.036	0.031	0.101
Mean AE right rotation (°)	0.231	0.476	0.476	0.448	0.483	0.154
<i>p</i> -value	0.471	0.118	0.117	0.145	0.112	0.633

Spearman rho correlation coefficients are reported, * sig at 0.05 level, ** sig after Bonferroni correction (0.05/6=0.0083)

AE: absolute joint repositioning error, ML: medio-lateral direction, AP: antero-posterior direction, mean Vel: mean velocity of the CoP displacement, Area: area of an ellipse that encompassed 95% of the CoP distribution

3

4

1 **Discussion**

2 Postural control during quiet sitting in patients with adult-onset idiopathic CD was compared
3 with healthy controls. Secondary, the influence of cervical sensorimotor control and disease
4 characteristics were investigated. The data showed that all CoP parameters were increased in
5 patients with and without head tremor compared to the control group. Patients with a dystonic head
6 tremor showed a larger postural sway and higher sway velocity than patients without a head tremor.
7 In a stable sitting position, the area of the CoP displacement is 4 times larger in patients without
8 head tremor than in controls. The impaired postural control was strongly correlated with
9 impairments in cervical sensorimotor control, not with disease specific characteristics. Impairments
10 in cervical sensorimotor control were not different between patients with or without head tremor.
11 We assume patients with head tremor were able to maintain their head still for a short moment
12 when repositioning measurements were obtained.

13 Previous posturographic reports in quiet stance showed conflicting results. Two studies
14 reported no differences in postural sway in stance between healthy controls and patients with CD
15 (Lekheli et al. 1997; Moreau et al. 1999). Contrary, 2 studies reported that several parameters of
16 postural sway were enlarged in patients with CD (Wöber et al. 1999; Bove et al. 2007). Sway path,
17 sway area as well as medio-lateral and antero-posterior displacements were enlarged. Differences in
18 patient inclusion might have contributed to these contradictory results. The latter included patients
19 with a dystonic head tremor whereas the first studies excluded patients with head tremor. It is
20 therefore not clear whether the enlarged postural sway might be induced by the presence of head
21 tremor. For this reason, the patient group in this study was subdivided based on the presence of
22 head tremor. Our findings show that head tremor is not the sole explanation for impaired postural
23 control as patients without head tremor also showed significantly larger postural sway parameters
24 compared to asymptomatic controls.

1 This is the first study to investigate postural control in a sitting posture. The increased
2 postural sway suggests higher susceptibility to postural instability. Even in a stable seated condition,
3 the postural sway of both patients with and without dystonic head tremor is enlarged. Different
4 explanations should be considered. First, somatosensory input from the neck is altered in CD. Our
5 data show that patients have impaired cervical sensorimotor control. These findings corroborate
6 previous research in which impairments in somatosensory integration and muscle spindle afference
7 have been observed (Tinazzi et al. 2003; Konczak and Abbruzzese 2013). The strong correlation
8 between postural sway and impaired cervical sensorimotor control leads to the assumption that the
9 altered somatosensory input from the neck might contribute to impaired postural control. We found
10 no difference between the eyes open and eyes closed condition. Therefore, patients do not
11 predominantly rely on visual input for postural control in a seated position. As vestibular function
12 seems to be intact in CD (Rosengren and Colebatch 2010), we assume that impaired cervical
13 sensorimotor control resulted in the larger postural sway. This might seem contradictory to previous
14 research where upright stance is not affected by neck muscle vibration in patients with CD. Patients
15 seemingly ignored the sensory afference from the muscle spindles so that postural sway in stance
16 was not affected by neck muscle vibration (Wöber et al. 1999; Bove et al. 2007). In stance, ankle
17 strategy is predominantly used to maintain postural control (Gatev et al. 1999). In this study, patients
18 sat in a stable position thus limiting the contribution of somatosensory afferent input and balance
19 strategies of the lower limbs. This might imply that in the sensory weighting processes during
20 postural control, the dependence on somatosensory input from the trunk and neck increased
21 (Peterka 2002; Putzki et al. 2006). This might explain the distinct difference found in this study
22 between healthy controls and patients with CD. Second, centrally impaired somatosensory
23 processing might contribute to loss of postural control (Tinazzi et al. 2009). Moreover, CD has been
24 attributed to dysfunction of the basal ganglia and its connections with the cerebellum (Berardelli et
25 al. 1998; Neychev et al. 2011; Quartarone and Hallett 2013; Prudente et al. 2014). As the basal
26 ganglia generate and maintain movement by co-activation of agonist-antagonist muscles to maintain

1 balance (Zahra 2013), impairments in basal ganglia and cerebellum may disturb posture (Takakusaki
2 2017). We suspect that postural control is inherently affected in CD as there was no correlation
3 observed between the enlarged postural sway and disease severity. Our findings add to the evidence
4 for impaired postural control in CD (Wöber et al. 1999; Bove et al. 2007; Barr et al. 2017).

5 The presence of dystonic head tremor resulted in larger postural sway amplitude and velocity
6 in patient with a dystonic head tremor compared to patients without head tremor and healthy
7 controls. This might suggest these patients are even more susceptible for balance problems. The
8 larger postural sway might be attributed to alterations in visual input. It is unclear whether gaze
9 stability is impaired in patients with a dystonic head tremor. The vestibulo-ocular reflex (VOR)
10 appears to be intact in patients without head tremor (Rosengren and Colebatch 2010) and suspect
11 that VOR adaptation occurs in long term dystonic head tremor. Bove and co-workers however (Bove
12 et al. 2006) suggested that the inability to focus on one point in patients with essential head tremor
13 might affect postural steadiness. As they observed a larger sway path in patients with essential head
14 tremor compared to patients with essential tremor affecting the arm(s). In this study however, we
15 did not find a difference in the eyes open and eyes closed condition in patients with head tremor. On
16 the contrary, postural sway tended to decrease in the eyes closed condition. We therefore assume
17 that visual dependence is rather low or patients used a stiffening strategy because of the increased
18 difficulty of the task (Field et al. 2008). Secondly, the enlarged postural sway amplitude and velocity
19 might merely be a reflection of the head tremor. The amplitude and velocity of head movements
20 during the dystonic head tremor might (mechanically) have enlarged the CoP displacements although
21 patients tried to keep the head as still as possible. When patients with CD keep their head still on
22 target, 2 subtypes of dystonic head tremor have been described by Shaikh et al. (2013). One subtype
23 with a large amplitude and low frequency with a jerky quality caused by slow movement in one
24 direction and a faster corrective movement in the opposite direction. A second subtype showed a
25 small amplitude and high frequency similar to essential tremor. The patients in our sample showed
26 the first subtype: a visible head tremor with a large amplitude. As the corrective phase of the

1 dystonic tremor has a high velocity, part of the higher CoP velocity found in our data might be
2 attributed to the head tremor. Similarly, part of the larger stabilometric parameters (path, area,
3 medio-lateral and antero-posterior range) found in patients with head tremor might be attributed to
4 the tremor and not solely to impaired postural steadiness. Further research might clarify these
5 findings.

6 The proportion of patients with head tremor in our sample is comparable to other research
7 (van den Dool et al. 2016). The small number of patients in the 2 subgroups limit the power of the
8 results. Nevertheless, the significant increased postural sway amplitude and velocity indicate a
9 potential negative impact of CD on postural control.

10 Gender could be a potential source of bias. Since the prevalence of CD is higher in females
11 with a reported female/male ratio of 2:1 (Steeves et al. 2012; Defazio et al. 2013), a higher
12 percentage of females was included in the patient group compared to the control group. However,
13 no gender differences have been reported for cervical sensorimotor control (Artz et al. 2015; de Vries
14 et al. 2015) and we could not find research reporting gender differences in seated postural control.
15 We therefore believe gender did not affect our results.

16 In conclusion, postural sway is doubled during quiet sitting in patients with CD. Our data add
17 to the yet limited reports on impaired postural control in CD. The alterations in somatosensory input
18 from the neck or somatosensory processing might contribute to a decrease in postural control.
19 Impairments in postural control during sitting might affect everyday life activities for example the
20 ability to read or working on the computer. Not only the deviated head position but also a decrease
21 in postural steadiness might complicate the task. The findings provide rationale to not limit the
22 physical therapy approach to neck impairments but to explore different modalities such as postural
23 control.

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4 **Conflict of interest:**

5 The authors declare that they have no conflict of interest.

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