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Doxorubicin induces arterial stiffness: a comprehensive *in vivo* and *ex vivo* evaluation of vascular toxicity in mice

- 3 Matthias Bosman¹, Kasper Favere^{1, 2, 3, 4}, Cédric H.G. Neutel¹, Griet Jacobs¹, Guido R.Y. De Meyer⁵, Wim
- 4 Martinet⁵, Emeline M. Van Craenenbroeck^{2, 4} and Pieter-Jan D.F. Guns¹
- ¹ University of Antwerp, Faculty of Medicine and Health Sciences, Laboratory of Physiopharmacology, Campus
 Drie Eiken, Universiteitsplein 1, B-2610, Antwerp, Belgium
- 7 ² University of Antwerp, Research Group Cardiovascular Diseases, GENCOR, Antwerp, Belgium
- ³ Ghent University, Faculty of Medicine and Health Sciences, Department of Internal Medicine, C. Heymanslaan
 10, B-9000, Ghent, Belgium
- ⁴ Antwerp University Hospital (UZA), Department of Cardiology, Drie Eikenstraat 655, B-2650, Edegem,
 Belgium
- ⁵ University of Antwerp, Faculty of Pharmaceutical, Biomedical and Veterinary Sciences, Laboratory of
 Physiopharmacology, Campus Drie Eiken, Universiteitsplein 1, B-2610, Antwerp, Belgium

Corresponding author: Matthias Bosman: University of Antwerp, Faculty of Medicine and Health Sciences,
 Laboratory of Physiopharmacology, Campus Drie Eiken, Universiteitsplein 1, B-2610, Antwerp, Belgium. E mail: matthias.bosman@uantwerpen.be

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- Figure 5 & 7 are preferably displayed in colour online; all other figures can be shown in greyscale.

24 ABBREVIATIONS

- aaPWV = abdominal aorta pulse wave velocity
- ACh = acetylcholine
- 27 cfPWV = carotid femoral pulse wave velocity
- 28 DEANO = diethylamine NONOate
- 29 DOX = doxorubicin
- EC(s) = endothelial cell(s)
- 31 eNOS = endothelial nitric oxide synthase
- 32 L-NAME = $N\omega$ -nitro-L-arginine methyl ester
- 33 LVEF = left ventricular ejection fraction; LVAW = left ventricular anterior wall; LVID = left ventricular
- 34 internal diameter; LVPW = left ventricular posterior wall
- 35 NO = nitric oxide
- 36 PE = phenylephrine
- 37 ROTSAC = Rodent Oscillatory Tension Set-up to study Arterial Compliance
- **38** VSMC(s) = vascular smooth muscle cell(s)

39 ABSTRACT

40 Arterial stiffness is an important predictor of cardiovascular risk. Clinical studies have demonstrated that arterial 41 stiffness increases in cancer patients treated with the chemotherapeutic doxorubicin (DOX). However, the 42 mechanisms of DOX-induced arterial stiffness remain largely unknown. This study aimed to evaluate artery 43 stiffening in DOX-treated mice using in vivo and ex vivo techniques. Male C57BL/6J mice were treated for 2 44 weeks with 2 mg/kg (low dose) or 4 mg/kg (high dose) of DOX weekly. Arterial stiffness was assessed in vivo 45 with ultrasound imaging (abdominal aorta pulse wave velocity (aaPWV)) and applanation tonometry (carotid-46 femoral PWV) combined with ex vivo vascular stiffness and reactivity evaluation. The high dose increased 47 aaPWV, while cfPWV did not reach statistical significance. Phenylephrine (PE)-contracted aortic segments 48 showed a higher Peterson's modulus (Ep) in the high dose group, while Ep did not differ when vascular smooth 49 muscle cells (VSMCs) were relaxed by a NO donor (DEANO). In addition, aortic rings of DOX-treated mice 50 showed increased PE contraction, decreased basal nitric oxide (NO) index and impaired acetylcholine-induced 51 endothelium-dependent relaxation. DOX treatment contributed to endothelial cell loss and reduced endothelial 52 nitric oxide synthase (eNOS) expression in the aorta. In conclusion, we have replicated DOX-induced arterial 53 stiffness in a murine model and this aortic stiffness is driven by impaired endothelial function, contributing to 54 increased vascular tone.

55 KEY WORDS

56 Arterial stiffness, doxorubicin, endothelial dysfunction, cardio-oncology, cardiovascular toxicity

57 1. INTRODUCTION

58 Large artery stiffening is an important feature in the process of vascular ageing [1, 2]. Under physiological 59 conditions, the heart ejects blood from the left ventricle into the aorta at high velocity [2]. The distensibility of the 60 aorta during systole will mitigate the increase in aortic pressure, while the elastic recoil during diastole supports 61 blood flow [3-5]. In contrast, arterial stiffening impairs the dampening capacity of the aorta, which, in turn, leads 62 to increased afterload on the heart and increased pulsatility in highly perfused organs, such as the kidneys, brain 63 and heart, potentially damaging them [6]. In previous studies, stiffening of the aorta has been associated with 64 increased risk of developing coronary artery disease, atrial fibrillation, stroke and heart failure [7-9]. Hence, 65 arterial stiffness, measured non-invasively by pulse wave velocity (PWV), is an early and predictive marker of 66 future cardiovascular events [10].

67 For a long time, research has mainly focussed on structural changes contributing to arterial stiffness, such as the 68 balance between collagen synthesis and elastin degradation within the vascular wall [11-13]. Although structural 69 remodelling is an important contributor to vascular ageing, there is emerging evidence that artery stiffening is 70 regulated by active components as well. More specifically, endothelial cells (ECs) and vascular smooth muscle 71 cells (VSMCs) have been reported to contribute to arterial stiffness by dysregulating vascular tone [14, 15]. For 72 example, decreased nitric oxide (NO) bioavailability and elevated contraction are associated with increased aortic 73 stiffness [16, 17]. Therefore, large artery stiffening depends on a delicate, not mutually exclusive, balance between 74 these active and passive elements.

75 In humans, carotid-femoral pulse wave velocity (cfPWV) assessed by tonometry is the gold-standard method for 76 evaluating arterial stiffness, but in mice ultrasound imaging is more frequently used [18, 19]. Ultrasound imaging 77 offers a local determination of aorta PWV, such as abdominal aorta PWV (aaPWV) [20], while tonometry focusses 78 more on regional determination of PWV [21]. These in vivo techniques offer a high translational value, but do not 79 provide insight about the underlying active and passive mechanisms that are involved. In addition, in vivo 80 measurements are dependent on heart rate and blood pressure [22]. Therefore, we have established a unique in-81 house developed organ bath set-up, called the Rodent Oscillatory Tension Set-up to study Arterial Compliance 82 (ROTSAC), to assess arterial stiffness ex vivo, independent from confounding factors, such as heart rate and blood 83 pressure [17, 23, 24].

84 Here we present a preclinical study investigating arterial stiffness in mice treated with doxorubicin (DOX). DOX 85 is a chemotherapeutic of the class of anthracyclines that is used to treat a wide variety of cancers, such as breast 86 cancer, lymphoma and haematological malignancies [25]. However, dose-dependent cardiotoxicity limits the 87 clinical use of DOX [26]. The mechanisms of DOX-induced cardiotoxicity have been intensively investigated 88 (reviewed elsewhere) [26], yet the effects on the vascular system have been less considered. Clinical studies have 89 shown increased arterial stiffness after DOX-therapy. Moreover, some childhood cancer survivors show signs of 90 accelerated cardiovascular ageing as well [27-30]. In murine models, DOX contributes to EC and VSMC dysfunction [31, 32]. More specifically, DOX mediates excessive reactive oxygen species (ROS) production, 91 92 which might impair NO signalling, thereby disturbing endothelium-dependent vasodilation ex vivo [33]. 93 Furthermore, low doses of DOX induce senescence of VSMCs in vitro, contributing to vascular damage [34]. 94 However, it remains unclear whether increased arterial stiffness in DOX-treated patients is caused by an altered 95 vascular tone or by structural remodelling. Therefore, the current study aimed to replicate DOX-induced arterial 96 stiffening in a preclinical murine model and to delineate the mechanisms involved herein.

97

2. MATERIALS & METHODS

98 2.1 Animals & Ethical approval

99 24 male C57BL/6J mice (Charles River, France) between an age of 10 and 12 weeks and with a body weight 100 between 26 and 30 g were housed in the animal facility of the University of Antwerp in standard cages with 12-12 hours light-dark cycles with access to regular chow and water *ad libitum*. Male mice were chosen to avoid the 102 influence of female hormone confounding factors. The experiments were approved by the Ethical Committee of 103 the University of Antwerp and were conform to the ARRIVE guidelines and to the Guide for the Care and Use of 104 Laboratory Animals published by the US National Institutes of Health (NIH Publication no.85-23, revised 1996).

105

2.2 DOX treatment and experimental workflow

106 Mice were randomly divided into three groups: vehicle (n = 8), low dose DOX (2 mg/kg; n = 8) and high dose 107 DOX (4 mg/kg; n = 8). DOX was injected intraperitoneally once per week for a total of two weeks. DOX 108 (Adriamycin®, 2 mg/mL) was diluted in a 0.9% NaCl solution (B. Braun, Belgium) on the day of injection. The 109 vehicle group received an intraperitoneal injection (10 mL/kg) of a 0.9% NaCl solution. Ultrasound imaging was 110 performed before (day -1) and 4, 7 and 11 days after the start of DOX treatment. The time points were selected 111 based on a pilot study where mice were measured daily after treatment with a high dose of DOX (data not shown). 112 Applanation tonometry and blood pressure were evaluated on day 5 and 10, respectively, after starting DOX 113 treatment. Mice were sacrificed between 12 and 13 days after the start of treatment for ex vivo measurements with 114 ROTSAC and organ baths. Supplementary figure 1 provides an overview of the experimental design and 115 workflow.

116

2.3 High-frequency ultrasound imaging

117 Ultrasound imaging was performed in anaesthetised mice under 1.5 - 2.5% (v/v) isoflurane (Forene; Abbvie, 118 Belgium) using a high-frequency ultrasound system (Vevo2100, VisualSonics). Images were only acquired when 119 heart rate and body temperature met the inclusion criteria, i.e. 550 ± 50 beats/min and 37 ± 1 °C, respectively. M-120 mode images were obtained for determination of cardiac parameters using a 24-MHz transducer. Left ventricular 121 ejection fraction (LVEF), left ventricular internal diameter (LVID), stroke volume, left ventricular anterior wall 122 (LVAW) and left ventricular posterior wall (LVPW) thickness were subsequently calculated using measurements 123 of three consecutive M-mode cycles with Vevo LAB Software (Version 3.2.0, VisualSonics). In the same session, 124 abdominal aorta PWV (aaPWV) was determined according to the method developed by Di Lascio et al. with a 125 24-MHz transducer [20]. Briefly, pulse wave Doppler tracing was used to measure aortic flow velocity (V). Immediately thereafter, aortic diameter (D) was measured on 700 frames-per-second B-mode images of the
abdominal aorta in EKV imaging mode. The ln(D)-V loop method was then applied to calculate aaPWV, using
MathLab v2014 software (MathWorks).

129 **2.4** Applanation tonometry

130 Carotid-femoral PWV (cfPWV) was determined in anaesthetised mice (4 - 6% sevoflurane (v/v) (Sevorane; 131 Abbvie, Belgium), as previously described by our research group [21]. In brief, two pulse tonometers (SPT-301, 132 Millar Instruments) were applied on the skin using a micromanipulator. Carotid–femoral transit time (Δt) was 133 determined using the time difference between the foot of carotid and femoral artery pulses (foot-to-foot method). 134 The foot of the pressure wave was defined as the second derivative maximum. Fifty consecutive pulses with 135 sufficient amplitude and a reproducible waveform were analysed; pulses that interfered with respiratory 136 movement peaks were excluded.

137 2.5 Blood pressure evaluation

Systolic and diastolic blood pressure were determined at day 10 non-invasively in restrained, awake mice using a
tail-cuff system with programmed electrosphygmomanometer (Coda, Kent Scientific Corporation). To reduce
stress and variability during the procedure, animals were trained for two days prior to the actual measurements.

141 2.6 *Ex vivo* evaluation of aortic stiffness and vascular reactivity

Mice were intraperitoneally injected with sodium pentobarbital (75 mg/kg; Sanofi, Belgium), followed by perforation of the diaphragm (when under deep anaesthesia). The thoracic aorta was carefully dissected and cut into six segments of 2 mm length (i.e. TA0 to TA5) with the crossing of the diaphragm as the reference point for the sixth segment (TA5). Next, segments were mounted between two hooks of an *ex vivo* organ bath set-up (10 mL) filled with Krebs Ringer solution (37°C, 95% O2/5% CO2, pH 7.4) containing (in mmol/L): NaCl 118, KCl 4.7, CaCl2 2.5, KH2PO4 1.2, MgSO4 1.2, NaHCO3 25, CaEDTA 0.025, and glucose 11.1.

For ROTSAC: *Ex vivo* assessment of arterial stiffness was performed as previously described [23]. In brief, segments (TA2 and TA3) were continuously stretched between alternating preloads corresponding to "systolic" and "diastolic" transmural pressures and at a physiological frequency of 10 Hz to mimic the physiological heart rate in mice (600 beats/ min). The set-up is calibrated by acquiring photographs of each aorta segment at different tensions (10 to 60 mN), from which the diameter and width of the segment are determined. Subsequently, these parameter serve as input in the LaPlace's equation to calculate in real-time the "systolic" and "diastolic" pressure and the Peterson's modulus (Ep), a measure for arterial stiffness. Ep was calculated as follows: Ep = $D_0 * \Delta P / \Delta D$ with ΔP = difference in pressure (kept constant at 40 mmHg), D_0 = "diastolic" diameter and ΔD = the change in diameter between "diastolic" and "systolic" pressure.

157 The ROTSAC protocol included the evaluation of arterial stiffness (Ep) at different pressures (i.e. 60-100, 80-158 120, 100-140 and 120-160 mmHg). Furthermore, the contribution of VSMC tonus was investigated by adding a 159 high concentration (2 μ M) of the α 1-adrenergic receptor agonist phenylephrine (PE), while the contribution of 160 ECs was evaluated by blocking endothelial nitric oxide synthase (eNOS) with Nω-nitro-L-arginine methyl ester 161 (L-NAME, 300 μ M). Conversely, a high concentration (2 μ M) of the NO-donor diethylamine NONOate 162 (DEANO) was added to completely relax VSMCs to remove vascular tonus, which allows the evaluation of 163 passive stiffness of the vessel wall. The detailed protocol for the ROTSAC experiments is provided in 164 supplementary figure 2.

165 For organ baths with isometric transducer: aortic segments (TA4 and TA5) were mounted at a preload of 20 mN. 166 Since we have previously shown that basal NO declines over time [35], the experimental protocol was started 70 167 minutes after puncture of the diaphragm to minimise time-dependent biases. VSMC contraction was evaluated by 168 adding cumulative concentrations of PE (3 nM - 10 μ M). Additionally, the basal NO index was calculated as 169 follows: PE was first added to induce VSMC contraction (PE contraction). Once the contraction was stable, the 170 eNOS blocker L-NAME (PE + L-NAME contraction) was subsequently added, further increasing contraction. By 171 substracting the PE contraction from the PE + L-NAME contraction, the amount of contraction that is solely due 172 to L-NAME (eNOS inhibition) can be acquired, which provides an estimate of basal NO. Endothelium-dependent relaxation was investigated by addition of cumulative concentrations of acetylcholine (ACh), a muscarinic 173 174 receptor agonist. The involvement of Ca²⁺-channels was determined by adding a single, high concentration (35 175 μ M) of diltiazem, a voltage-gated Ca²⁺-channel blocker. The detailed protocol for the organ bath experiments and 176 the method for basal NO index calculation is illustrated in supplementary figure 3.

177 2

2.7 Chemical compounds

- 178 DOX (Adriamycin®, 2 mg/mL) was purchased from Pfizer (Belgium). PE, L-NAME, ACh, DEANO and
 179 diltiazem were purchased from Sigma-Aldrich (Belgium).
- 180

181

2.8 Histology

183 Aortic segments were fixed in 4% formalin for 24 h, dehydrated overnight in 60% isopropanol and then embedded 184 in paraffin. Transversal sections were stained with orcein or immunohistochemically stained with a primary 185 antibody against collagen type I (1:500; ab21286, Abcam) to determine elastin and collagen type I content, 186 respectively. The EC layer continuity was evaluated with immunohistochemical staining with a primary antibody 187 against CD31 (1:100; D8V9E, Cell Signalling Technology) and visualised with EnVision+ (Dako). Images were 188 acquired with Universal Graph 6.1 software using an Olympus BX40 microscope and quantified with ImageJ 189 software. Elastin and collagen type I content were quantified by calculating the signal-to-wall area ratio 190 (expressed as percentage). CD31 was quantified by determining the length of CD31 positive cells along the 191 luminal border divided by the total aortic lumen circumference (expressed as percentage).

192 **2.9** Western blotting

193 Aortic samples were lysed in Laemmli sample buffer (Bio-Rad) containing 5% β-mercaptoethanol (Sigma-194 Aldrich) and subsequently heat-denatured for 5 minutes at 100 °C. Next, samples were loaded on Bolt 4–12% 195 Bis-Tris gels (Invitrogen) and after electrophoresis transferred to Immobilon-FL PVDF membranes (Millipore) 196 according to standard procedures. Thereafter, membranes were immediately blocked for 1 hour in Odyssey Li-197 COR blocking buffer. After blocking, membranes were probed with primary antibodies, diluted in Odyssey Li-198 COR blocking buffer, overnight at 4 °C. The following primary antibodies were used: mouse anti-eNOS (1:500; 199 ab76198, Abcam) and mouse anti-β-actin (1:5000; ab8226, Abcam). The next day, membranes were incubated 200 with IRDye-labeled secondary antibodies (goat anti-rabbit IgG926-32211; goat anti-mouse IgG926-68070, both 201 purchased from Li-COR Biosciences) for 1 hour at room temperature. Membranes were visualised with an 202 Odyssey SA infrared imaging system (Li-COR Biosciences). Western blot data was quantified using ImageJ 203 software. Signal intensity of the protein of interest (eNOS) was normalised to the β-actin signal intensity and 204 expressed as the fold change (compared to vehicle).

205 2.10 Statistical analysis

All results were expressed as the mean \pm standard error of the mean (SEM). Statistical analyses were performed using GraphPad Software (Prism 8 - Version 8.4.2, Graphpad, USA). Repeated measures two-way ANOVA, oneway ANOVA and Kruskal-Wallis tests were performed for comparison between groups. A Dunnett's post hoc test was used to correct for multiple comparisons. A Bland-Altman plot was used to evaluate concordance between aaPWV (day 4 and 7) and cfPWV (day 5) values. A p-value < 0.05 was considered to be statistically significant.

211 **3. RESULTS**

212

2 3.1 DOX (high dose) increased aaPWV in vivo

A significant and consistent increase in aaPWV was observed for the high dose group at 4, 7 and 11 days after the start of DOX treatment (Figure 1A). More specifically, at 4, 7 and 11 days, aaPWV was 5.67 ± 0.32 m/s, $5.36 \pm$ 0.30 m/s and 5.034 ± 0.25 m/s in the high dose group compared to 4.36 ± 0.31 m/s, 4.00 ± 0.24 m/s and $4.13 \pm$ 0.20 m/s in the vehicle group, respectively (Figure 1A). LVEF did not differ among treatment groups (Figure 1B). Additional evaluated cardiovascular parameters, including LVAW, LVID, LVPW, stroke volume, heart mass and body weight (measured at day 11) are provided in Table 1. These parameters did not change between the different treatment groups after DOX treatment (Table 1), except pulse pressure. Pulse pressure, the difference between

systolic and diastolic blood pressure, was significantly elevated in the high dose group (Table 1).



221



227 Table 1: Additional cardiovascular parameters	and body	weight.
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	Vehicle	Low Dose (2 mg/kg)	High Dose (4 mg/kg)
LVAW thickness systole (mm)	1.20 ± 0.07	1.20 ± 0.05	1.19 ± 0.04
LVAW thickness diastole (mm)	0.78 ± 0.03	0.76 ± 0.03	0.77 ± 0.03
LVID systole (mm)	1.86 ± 0.06	1.90 ± 0.12	2.05 ± 0.06
LVID diastole (mm)	3.33 ± 0.07	3.18 ± 0.13	3.48 ± 0.06
LVPW thickness systole (mm)	1.50 ± 0.07	1.46 ± 0.03	1.53 ± 0.04
LVPW thickness diastole (mm)	0.91 ± 0.05	0.96 ± 0.08	0.90 ± 0.03
Stroke volume (µL)	33.8 ± 1.73	29.3 ± 2.27	36.65 ± 1.64
Heart mass (mg)	143.2 ± 6.1	139.9 ± 1.9	133.7 ± 4.4
Body weight (g)	27.8 ± 0.8	27.2 ± 0.9	25.8 ± 0.8
Systolic blood pressure (mmHg)	103 ± 4	104 ± 4	105 ± 3
Diastolic blood pressure (mmHg)	77 ± 3	74 ± 5	72 ± 3
Pulse pressure (mmHg)	26 ± 2	30 ± 1	$33 \pm 2 *$

228Abbreviations: LVAW, left ventricular anterior wall; LVID, left ventricular internal diameter; LVPW, left ventricular posterior229wall. * p < 0.05 compared to vehicle. For vehicle: n = 8, low dose: n = 8 and high dose: n = 8. (2-column fitting table)

Measurement with tonometry, only performed at day 5 for logistical reasons, showed a trend (p = 0.0547) of increased cfPWV in the high dose group (Figure 2A). Individual aaPWV-values for all time points are presented in Figure 2B to illustrate inter-animal variability. To evaluate the agreement between aaPWV and cfPWV measurement techniques a Bland-Altman plot was created. Bland-Altman analysis revealed that aaPWV values were systematically higher than cfPWV values (bias = 1.372) (Figure 2C). In addition, the bias tended to be higher with increasing PWV values (Figure 2C).





Figure 2: *In vivo* measurement of cfPWV in vehicle-, low dose- and high dose-treated mice and comparison of aaPWV and cfPWV. cfPWV in the high dose group did not significantly increase compared to the vehicle group (p = 0.0547) (A).
aaPWV values were systematically higher than cfPWV values after Bland-Altman analysis (bias = 1.372) (B & C). For vehicle:
n = 8, low dose: n = 8 and high dose: n = 8. For A: One-way ANOVA with Dunnett's multiple comparisons test. For B:
Repeated measures two-way ANOVA with Dunnett's multiple comparisons test. For B:
represent 95% limits of agreement) *, ** p < 0.05, 0.01. (2-column fitting image)

243

244 3.2 DOX (high dose) increased aortic stiffness *ex vivo*

The "diastolic" and "systolic" diameters (at 80 –120 mmHg) in Krebs Ringer and PE conditions, determined in the *ex vivo* ROTSAC set-up, are presented in figure 3A and 3B, respectively. The change (Δ) in "systolic" and "diastolic" diameter after PE-addition as compared with Krebs Ringer conditions was calculated (Figure 3C). This Δ diameter corresponds with the magnitude of contraction. In the high dose group, the change in "systolic" and "diastolic" diameter increased significantly, reflecting higher PE-induced contractions. Low dose-treated animals showed a non-significant trend towards elevated contraction (Figure 3C).



Figure 3: Evaluation of "diastolic" and "systolic" diameters in the *ex vivo* ROTSAC set-up. Diastolic and systolic diameter in Krebs Ringer and PE conditions at 80-120 mmHg (A & B). Δ Diameter (Krebs - PE) was significantly increased in high dose-treated mice during systole and diastole (C). For vehicle: n = 8, low dose: n = 8 and high dose: n = 7. For C: Oneway ANOVA with Dunnett's multiple comparisons test. * p < 0.05 (2-column fitting image)



257 Ep, a measure of arterial stiffness, showed a pressure-dependent increase in all groups. Under Krebs Ringer 258 conditions, there was no significant difference in Ep between vehicle- and DOX-treated mice, both in the absence 259 and presence of L-NAME (300 µM) (Figure 4A & 4B). Similarly, in the presence of DEANO (2 µM), a NO-260 donor that removes vascular tonus, there were no differences in Ep between the vehicle and DOX-treated groups 261 (Figure 4C), indicating no alteration in passive stiffness. However, Ep was significantly increased in the high 262 dose-treated mice as compared with the vehicle-treated mice when aortic rings were stimulated with PE (2 µM) 263 (Figure 4D). Mice treated with the low dose of DOX did not exhibit a higher Ep value in the presence of PE 264 (Figure 4D). Remarkably, the high dose of DOX did not show a pressure-dependent increase in Ep in the combined 265 presence of PE and L-NAME. More specifically, mice treated with the high dose of DOX exhibited a lower Ep 266 value at 120 - 160 mmHg compared to the vehicle group (Figure 4E). 267 Furthermore, we determined the basal NO index by calculating the increase in Ep due to inhibition of eNOS with

L-NAME (Supplementary figure 2). The basal NO index (at 80-120 mmHg) was significantly decreased in the
high dose group as compared with the vehicle group (Figure 4F).

270 Finally, histological staining for elastin and collagen type I visualisation in aorta samples was performed to

- investigate potential structural remodelling (Figure 5). Elastin (Figure 5A) and collagen type I (Figure 5B) content
- did not differ between the treatment groups.
- 273





275 Figure 4: Assessment of aortic stiffness in mice treated with vehicle, low and high dose of DOX at different pressures 276 with the ex vivo ROTSAC set-up. Peterson's modulus (Ep), a measure for aortic stiffness, did not significantly differ between 277 vehicle- and DOX-treated mice in Krebs conditions in the absence and presence of L-NAME (A &B). Ep was similar in all 278 treatment groups in the presence of DEANO (C). Addition of 2 µM PE increased Ep in the high dose group compared to the 279 vehicle group (D). In the presence of PE (2 µM) combined with L-NAME (300 µM), the high dose group showed no pressure-280 dependency of Ep, resulting in a lower Ep at 120-160 mmHg (E). Basal NO index was significantly reduced the high dose 281 group (F). For vehicle: n = 8, low dose: n = 8 and high dose: n = 7. For A-E: Repeated measures two-way ANOVA with 282 Dunnett's multiple comparisons test. For F : One-way ANOVA with Dunnett's multiple comparisons test. *, ** p < 0.05, 283 <0.01 (2-column fitting image)



Figure 5: Evaluation of elastin and collagen type I content in the aortic wall of mice treated with vehicle, low and high dose of DOX. The elastin (A) and collagen type I (B) amount were not altered in the different treatment groups. For vehicle: n = 8, low dose: n = 8 and high dose: n = 8. For A and B: One-way ANOVA with Dunnett's multiple comparisons test (p > 0.05 for low and high dose compared to vehicle). Scale bar: $100 \,\mu$ M. (2-column fitting image)

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3.3 DOX impaired endothelium-dependent relaxation, basal NO index and increased contraction

The high dose group exhibited increased PE-induced contractions compared to the vehicle, while the low dose did not (Figure 6A). This difference disappeared in the presence of L-NAME (Figure 6A). The sensitivity of VSMCs for PE (defined by the EC₅₀) was significantly elevated in animals treated with the high dose of DOX (Figure 6B). More specifically, the mean EC₅₀-values (logarithmic) were -7.014 ± 0.050 M and -6.796 ± 0.052 M for the high dose and vehicle groups, respectively.

296 We further determined the basal NO index by calculating the change in isometric force due to eNOS-inhibition

297 with L-NAME (Supplementary figure 3). The basal NO index was significantly decreased in the high dose group

as compared with the vehicle group (Figure 6C).

299 ACh-induced endothelium-dependent relaxation was impaired (Figure 6D). Both the maximal relaxation and the

sensitivity for ACh was significantly reduced in the high dose-treated mice (Figure 6D & 6E). More specifically,

the mean EC₅₀-values (logarithmic) were -7.454 \pm 0.073 M and -7.751 \pm 0.086 M for the high dose and vehicle groups, respectively. In addition, there was no difference in DEANO-induced endothelium-independent relaxation between vehicle and DOX-treated mice nor in the sensitivity of VSMCs for DEANO (Figure 6D). For diltiazem (35 μ M), no differences in the magnitude of relaxation were present between the different groups (Figure 6F).



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306 Figure 6: VSMC and EC function in mice treated with vehicle, low and high dose of DOX determined in organ baths 307 with isometric force transducer. Concentration-response curves for mice treated with vehicle, low and high dose of DOX 308 under PE-stimulation in the absence and presence of L-NAME (A), ACh (D) and DEANO (D). Contraction and VSMC-309 sensitivity for PE increased significantly in high dose-treated mice compared to vehicle group (A & B), but not after addition 310 of L-NAME (A). Basal NO index, calculated from panel A, was significantly reduced in high-dose treated mice (C). No 311 changes were present in the magnitude of DEANO-induced relaxation (D). ACh-induced relaxation and sensitivity of the 312 endothelium for ACh decreased significantly in the high dose group (D & E). Diltiazem-induced relaxation did not differ 313 between treatment groups (F). For vehicle: n = 8, low dose: n = 8 and high dose: n = 8. For A and D: Repeated measures two-314 way ANOVA with Dunnett's multiple comparisons test. For B, C, E and F: One-way ANOVA with Dunnett's multiple 315 comparisons test. *, ** p < 0.05, <0.01 (2-column fitting image)

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173.4 DOX disrupted EC layer continuity and decreased eNOS-expression

318 Endothelial layer continuity and eNOS-expression in the aorta were further investigated. The EC layer was 319 evaluated with an immunohistochemical stain against CD31, a marker for ECs. CD31 positivity was significantly

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320 decreased in the high dose group compared to the vehicle in a dose-dependent way, revealing gaps in the EC

321 monolayer (Figure 7A). In addition, eNOS-expression was reduced in the high dose group as well (Figure 7B).



Figure 7: Evaluation of EC layer continuity with CD31 staining and eNOS-expression in mice treated with vehicle, low and high dose of DOX. CD31 staining revealed a significant dose-dependent decrease in EC layer continuity in the high dose group compared to the vehicle (A). In addition, high dose treatment with DOX reduced eNOS-expression (B). Panel A: Black arrows show discontinuity of the endothelial monolayer; For vehicle: n = 7, low dose: n = 8 and high dose: n = 8. Panel B: For vehicle: n = 6, low dose: n = 6 and high dose: n = 6. For A: One-way ANOVA with Dunnett's multiple comparisons test. For B: Kruskal-Wallis with Dunn's multiple comparisons test. * p < 0.05; Scale bar: 100 µM (2-column fitting image)

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4. DISCUSSION

Arterial stiffness is considered as an important predictor of cardiovascular disease [10]. While clinical studies
 have demonstrated an increase in arterial stiffness after DOX treatment, the exact mechanism remains elusive [27 30]. Here we present a study where DOX-induced arterial stiffness was investigated in mice, using both *in vivo*

- and *ex vivo* techniques.
- 335 The current study revealed a consistent increase in aaPWV after DOX treatment, while LVEF function remained
- unaffected. Previously, studies in mice demonstrated LVEF decline after DOX treatment, but these studies used
- high doses (20-25 mg/kg) [36, 37]. We used lower doses of DOX (8 mg/kg cumulative), since we did not aim to
- induce severe cardiotoxicity. Body weight and cardiac parameters were not altered after DOX treatment. The

339 observation of DOX-induced arterial stiffness in the absence of cardiac dysfunction is an important finding. Not 340 only does this indicate that the observed vascular toxicity during DOX treatment was independent of cardiac 341 parameters, but this also suggests that DOX-induced arterial stiffness either precedes DOX-cardiotoxicity, or 342 occurs at lower doses. In both cases, arterial stiffness holds potential as a clinical marker for identifying patients 343 at risk. Additionally, systolic and diastolic blood pressure did not significantly differ, but pulse pressure was 344 elevated in the high dose group, which may point to increased arterial stiffness [38]. The high dose (4 mg/kg) corresponds approximately with 160 mg/m² in patients, which is below the maximal recommended dose of 450 345 346 mg/m²[39, 40]. Furthermore, dosing schedules of DOX for breast cancer [41], non-Hodgkin lymphoma [42] and 347 small cell lung cancer [43] typically involve multiple DOX-infusions every 2 - 3 weeks. The doses used in our 348 preclinical study are also in line with epidemiological studies that have reported accelerated cardiovascular ageing 349 (i.e. increased vascular stiffness), especially in childhood cancer survivors [30].

350 In patients, regional cfPWV measured by applanation tonometry is the gold standard. In mice, cfPWV 351 measurements are feasible [21], but aaPWV by ultrasound imaging, is more frequently used. Although not the 352 primary objective of our study, we included a comparison between both methods. Bland-Altman analysis showed 353 that aaPWV in mice was consistently higher than cfPWV. aaPWV was more sensitive to detect DOX-induced 354 aortic stiffness in vivo in mice, although different timing of the methods and the use of a different anaesthetic do 355 not allow a direct head-to-head comparison. The absolute difference between the aaPWV and cfPWV values can 356 be attributed to variation in geometry and structure of the vessel wall along the arterial tree, which affects the 357 speed of the propagating pulse wave. Previous studies in humans have reported PWV values of 4.4 m/s, 6 m/s and 358 9 m/s at the aortic root, abdominal aorta and femoral artery, respectively [44, 45]. In this respect, cfPWV 359 represents an integrated average PWV of the different parts of the artery system [44, 45]. In addition, cfPWV 360 measurement depends on determination of the external carotid-femoral distance, which may be prone to a 361 measurement error, particularly in mice [21]. Taken together, these factors might explain the lower cfPWV values 362 and the observation of cfPWV not reaching statistical significance in the high dose group.

The *in vivo* data were confirmed in the *ex vivo* ROTSAC set-up. Aortic rings of high dose-treated mice showed significantly increased aortic stiffness, yet only in the presence of a contractile stimulus (PE). Hence, this finding suggests that a contractile stimulus, provided for example by catecholamines, is essential in the modulation of vascular tone after DOX treatment *in vivo*. Remarkably, in the presence of PE combined with L-NAME, high dose-treated animals showed no pressure-dependency of Ep compared to vehicle-treated animals. More specifically, half of the high dose-treated animals exhibited a decrease in Ep with increasing pressure (data not 369 shown), resulting in an apparent flattening of the Ep-pressure curve. The exact mechanism remains elusive, 370 although DOX has been shown to induce VSMC death and senescence in vitro [46, 47]. Another possible explanation may be the interaction of DOX with the extracellular environment or focal adhesion complexes, which 371 372 are required for maintaining vascular tonus [48]. Finally, DOX-related structural alterations were evaluated by adding a high dose of DEANO (2 μ M), an exogenous NO donor, which relaxes VSMCs and removes vascular 373 374 tone. In the absence of VSMC tonus, no difference in Ep was observed, which suggests unaltered passive stiffness 375 of the aortic wall. These findings were corroborated by histological stains for elastin and collagen type I, showing 376 no changes in elastin and collagen type I content. Hence, our results point towards active mechanisms contributing 377 to DOX-induced aortic stiffness.

378 Treatment with the high dose of DOX resulted in increased contraction force in response to PE, an α1-adrenergic 379 receptor agonist. In order to delineate the specific mechanisms involved herein, different aspects of vascular 380 function were further investigated. A dose response of DEANO was used to investigate endothelium-independent 381 relaxation of VSMCs. DEANO causes relaxation of VSMCs through a cyclic guanosine monophosphate (cGMP)-382 mediated pathway, which results in a reduction in free intracellular Ca²⁺, thus mediating relaxation of VSMCs 383 [49]. DEANO-induced relaxation did not differ between treatment groups, indicating unaltered guanylate cyclase 384 and cGMP-signalling. This suggests that the sensitivity of VSMCs for NO and the VSMC relaxation capacity 385 remain unaffected after DOX treatment We previously showed that PE causes an increase in intracellular Ca²⁺ through, in part, voltage-gated Ca^{2+} - channels, thus mediating contraction of VSMCs [50]. Therefore, using 386 387 diltiazem, a voltage-gated Ca2+-channel blocker, can provide useful insight about potential disturbed Ca2+-388 homeostasis involved in impaired VSMC contraction. Diltiazem-induced relaxation did not differ between the vehicle- and DOX-treated groups. This indicates that Ca2+-influx through voltage-gated calcium channels in 389 390 VSMCs is not perturbed in response to DOX-administration. Taken together, these findings show that VSMC-391 specific mechanisms involved in VSMC contraction and relaxation are not impaired. Hence, VSMC function 392 remains intact after DOX treatment.

The endothelial cell layer of the aorta plays a crucial role in regulating VSMC contraction and relaxation [51]. Low levels of basal NO are associated with endothelial dysfunction and, consequently, with increased VSMC contraction, contributing to aortic stiffness [16]. The basal NO index (percentage increase in PE-contraction upon addition of the eNOS blocker L-NAME) provides an estimate about basal NO production and thus is a useful marker for endothelial function. Previous work from our lab has demonstrated that in wild-type C57BL6 mice approximately 80% of maximal contraction (PE + L-NAME) is attributable to basal NO [35]. Contraction force was higher in the DOX-treated group upon PE-stimulation, but contraction force was similar between all treatment
groups after addition of L-NAME. Consequently, the index of basal NO was reduced in DOX-treated animals,
indicating that DOX potentially impairs NO production or NO bioavailability.

402 DOX treatment resulted in reduced CD31 positivity, reflecting gaps in the EC monolayer. This finding indicates 403 that DOX causes EC loss, probably through EC death. In addition, eNOS protein expression was decreased in the 404 high dose group. Both EC loss and reduced eNOS-expression may contribute to the observed decrease in basal 405 NO index, which, in turn, could result in endothelial dysfunction. The observed results are in line with a study of 406 He et al. (2019) in mice, that reported decreased EC viability and reduced eNOS-expression after 3 weeks of DOX 407 treatment (15 mg/kg cumulative) [52]. The authors identified excess ROS-accumulation after DOX treatment as 408 the primary cause of EC death and reduced eNOS expression, which resulted in decreased NO content [52]. DOX-409 induced ROS generation is mainly caused by the conversion of DOX in a superoxide radical via an intermediate 410 semiquinone structure at the reductase domain of eNOS [53]. Paradoxically, other studies have reported that eNOS 411 expression is upregulated in response to DOX due to ROS-accumulation [31, 54]. Moreover, DOX interferes with 412 eNOS function, resulting in uncoupling of eNOS [31, 54]. In this case, eNOS no longer produces NO, but instead, 413 contributes to superoxide formation, thereby exacerbating ROS-generation. However, these studies were 414 performed using a single high dose of doxorubicin (20 mg/kg) or were performed in vitro, which might explain 415 the difference between our results and these other studies.

416 Similarly, aortic rings of DOX-treated mice exhibited reduced endothelium-dependent relaxation. Previous work 417 from our research group has demonstrated that endothelial dysfunction increases vascular tone and thereby 418 actively augments arterial stiffness [17, 23, 55]. For instance, aortic segments of mice without eNOS expression 419 (eNOS^{-/-}) showed no endothelium-dependent relaxation, increased contraction and augmented arterial stiffness 420 [55]. Another recent study demonstrated reduced ACh-induced relaxation after DOX treatment (10 mg/kg 421 cumulative) in mice without altering relaxation in response to an exogenous NO-donor [33]. This is in agreement 422 with our results. However, impaired endothelium-independent relaxation by a NO-donor in mice after DOX 423 treatment (15 mg/kg cumulative) has also been reported [52]. While inactivation of NO by ROS has been proposed 424 as a possible mechanism [56], this concept is not supported by our DEANO relaxation curves, which were 425 identical for the three groups. Possibly, the mechanism of interference with NO signalling depends on the dose of 426 DOX. Our findings suggest that lower doses of DOX (< 15 mg/kg) decrease NO content by decreasing eNOS 427 expression, rather than inactivating NO with excess ROS.

In conclusion, we report a consistent increase in aaPWV in DOX treated mice, which was confirmed *ex vivo*.
Moreover, the *ex vivo* ROTSAC and organ bath experiments, revealed that exclusively active components are
involved in aortic stiffening in response to DOX. More specifically, DOX impaired endothelial function, resulting
in reduced endothelium-dependent relaxation and increased contraction, thereby augmenting arterial stiffness.
This endothelial dysfunction could be attributable to EC loss and reduced eNOS-expression. The experimental
DOX model and the methods presented in this study, offer the opportunity for further navigating the mechanisms
of arterial stiffening in DOX-treated patients.

435 AUTHOR CONTRIBUTIONS

436 M.B., G.J., E.V.C., G.D.M., W.M. and P.J.G. conceived and designed the experiments. Data acquisition, analysis,

437 and interpretation were carried out by M.B., K.F., C.N. and P.J.G.. The manuscript was drafted and critically

438 revised by M.B., K.F., C.N., G.J., G.D.M., W.M., E.V.C. and P.J.G. All authors have read and approved the final

439 version of the manuscript.

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447 CONFLICT OF INTEREST

448 The authors declare that the research was conducted in the absence of any commercial or financial relationships449 that could be construed as a potential conflict of interest.

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596 SUPPLEMENTARY FIGURES



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598 Supplementary figure 1: Experimental design and workflow. Male C57BL/6J mice were randomly divided 599 into three groups: a vehicle (n = 8), a low dose (n = 8) and a high dose group (n = 8). The low and high dose 600 groups received an intraperitoneal injection of 2 and 4 mg DOX/kg, respectively, once per week for a total of two 601 weeks. Ultrasound imaging for determination of aaPWV was performed at day -1 (baseline) and 4, 7 and 11 days 602 after the start of DOX treatment for all groups. Applanation tonometry for determination of cfPWV was only 603 performed at 5 days after the start of treatment. A blood pressure measurement was performed at day 10 (with 604 two training days at day 8 and 9). Mice were sacrificed and the aorta was removed for ex vivo ROTSAC and 605 isometric organ bath evaluation at 12 or 13 days after initiating DOX treatment.



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607 Supplementary figure 2: Experimental protocol for aortic stiffness evaluation in ROTSAC set-up. 608 Following calibration, Non-nitro-L-arginine methyl ester (L-NAME, 300 µM) was added to one segment to inhibit 609 endothelial nitric oxide synthase (eNOS) activity to investigate the basal NO index. After 15 minutes, Ep was 610 calculated for each pressure (from 60 - 100 mmHg to 120 - 160 mmHg). In order to investigate the active 611 contribution of VSMCs to DOX-induced aortic stiffness, phenylephrine (PE, 2 µM) was subsequently added to 612 the organ bath, followed by 15 minutes of incubation while keeping pressure constant at 80-120 mmHg. PE is a 613 selective agonist of al-adrenergic receptors on VSMCs and thereby initiates IP-3 mediated contraction. After 15 614 minutes, Ep was calculated for each pressure (from 60 - 100 mmHg to 120 - 160 mmHg). After washing 3x with 615 Krebs, diethylamine NONOate (DEANO, 2 μ M) was added to the organ bath and Ep was calculated for each 616 pressure (from 40 - 80 mmHg to 220 - 260 mmHg). DEANO is an exogenous NO-donor and induces endothelium-617 independent relaxation of VSMCs, thereby excluding VSMC tonus. This allows examination of the potential 618 contribution of passive elements to DOX-induced aortic stiffness.





620 Supplementary figure 3: Experimental protocol for vascular reactivity assessment in isometric organ baths.

First, increasing doses of PE were added to all segments with 2 minute intervals to investigate contractility force, followed by addition of L-NAME (300μ M) to 1 segment. Next, diltiazem (2μ M) was added to the organ bath to investigate the role of calcium channels in DOX-induced arterial stiffness. Diltiazem is a calcium-channel blocker, which inhibits calcium influx into the intracellular environment, thereby inhibiting contraction and inducing relaxation. After washing 3x with Krebs, the PE-dose response was repeated, followed by addition of increasing doses of acetylcholine (ACh) to the L-NAME-untreated segment and increasing doses of DEANO to the L-NAME-treated segment. ACh is a neurotransmitter that, when it binds to corresponding receptors on the

628 endothelium, induces relaxation of VSMCs. This allows examination of endothelial-dependent VSMC relaxation

and endothelial function in general.

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